

# An Interpretable Distance Measure for Multivariate Non-Stationary Physiological Signals

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## Introduction

**Motivation:** study of human locomotion [3]

- Angular velocity recorded on the left and right feet using a pair of sensors.
- Protocol: standing, walking, turning around, walking back, and standing.
- Multivariate signals with  $d = 16$  dimensions: norms of the STFT (Short Time Fourier Transform) of each univariate foot recording.

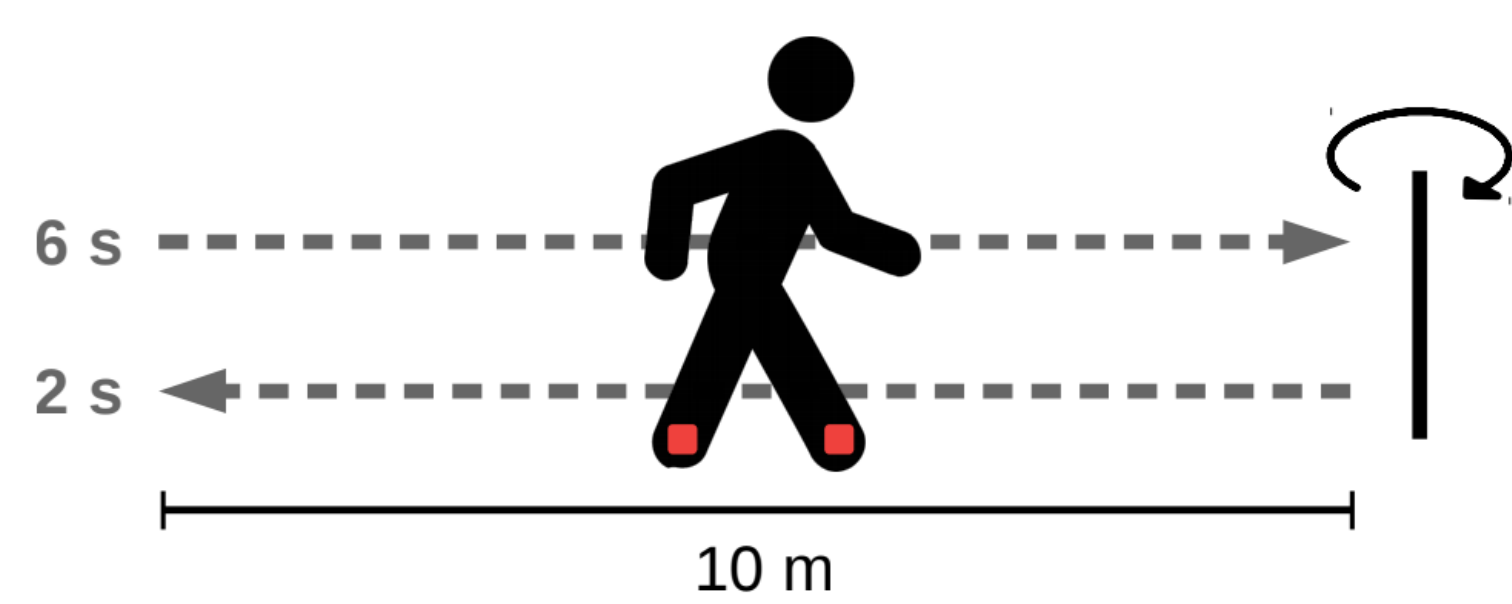


Figure 1: Gait signal acquisition protocol.

## Comparing multivariate time series

- Popular distances (Euclidean distance, Dynamic Time Warping) can not handle non-stationarity.
- Our distance is interpretable and can compare non-stationary signals: (i) symbolization, (ii) distance on strings.

## Symbolization technique

- 1 Segmentation step: a real-valued signal of length  $n$  is split into  $w$  segments ( $w < n$ ).
- 2 Quantization step: each segment is mapped to a discrete value taken from a set of  $A$  symbols.

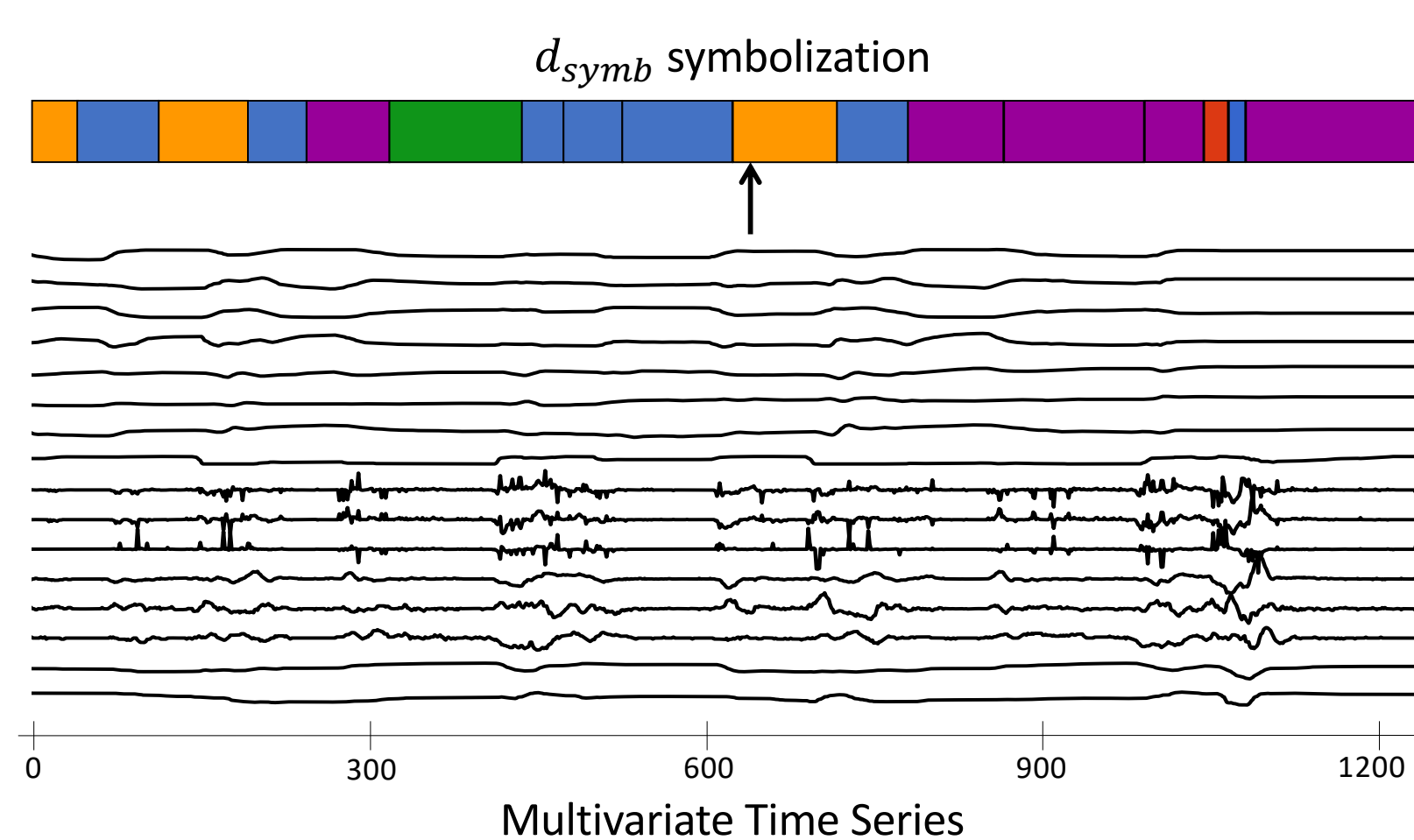


Figure 2: Symbolization of a multivariate signal into a string called a symbolic sequence (visualized using a color bar).

## Method: the $d_{symb}$ symbolization and distance measure

Steps of  $d_{symb}$  [1]

- 1 Segmentation: change-point detection (on the mean).
- 2 Quantization:  $K$ -means clustering (of the means per segment), with  $K = A$ .
- 3 Distance: general edit distance between the resulting symbolic signals.

### Change-point detection

Finding the  $w^*$  unknown instants  $t_1^* < t_2^* < \dots < t_{w^*+1}^*$  where the mean of signal  $x = (x_1, \dots, x_n)$  change abruptly:

$$(\hat{w}, \hat{t}_1, \dots, \hat{t}_{\hat{w}+1}) = \arg \min_{(w, t_1, \dots, t_{w+1})} \sum_{k=0}^{w+1} \sum_{t=t_k}^{t_{k+1}-1} \|x_t - \bar{x}_{t_k:t_{k+1}}\|^2 + \lambda w,$$

where  $\bar{x}_{t_k:t_{k+1}}$  is the empirical mean of  $\{x_{t_k}, \dots, x_{t_{k+1}-1}\}$  and  $\lambda > 0$  is a penalization parameter.

- Compromise between the reconstruction error and the number of change-points.
- When  $\lambda$  is small, many change-points are detected.
- For calibration purposes, we use  $\lambda = \ln(n)$ .
- Solved using the Pruned Exact Linear Time (PELT) algorithm [2], which is shown to have  $\mathcal{O}(n)$  complexity (under some assumptions).

### Levering the general edit distance

- 1 Preprocessing.
  - Including the segment length information: replicating each symbol proportionally to its segment length. Example: `abd` becomes `aabbbbdd`.
  - Shortening: dividing each length by the minimum length. Example: `aabbbbdd` becomes `abbd`.
- 2 Applying the general edit distance with custom costs.
  - Edit distance on strings (a.k.a Levenshtein distance): minimal cost of a sequence of operations that transform a string into another.
  - Allowed simple operations and their costs:
    - Substitution: Euclidean distance between the cluster centers of the symbols.
    - Insertion: max of substitution costs.
    - Deletion: max of substitution costs.
  - Total cost: sum of the costs of the simple operations.

## Experimental results: interpretation of the symbolization

The general structure is coherent with the clinical protocol: change-point detection finds stationary segments, and each symbol can be associated with a specific type of behavior.

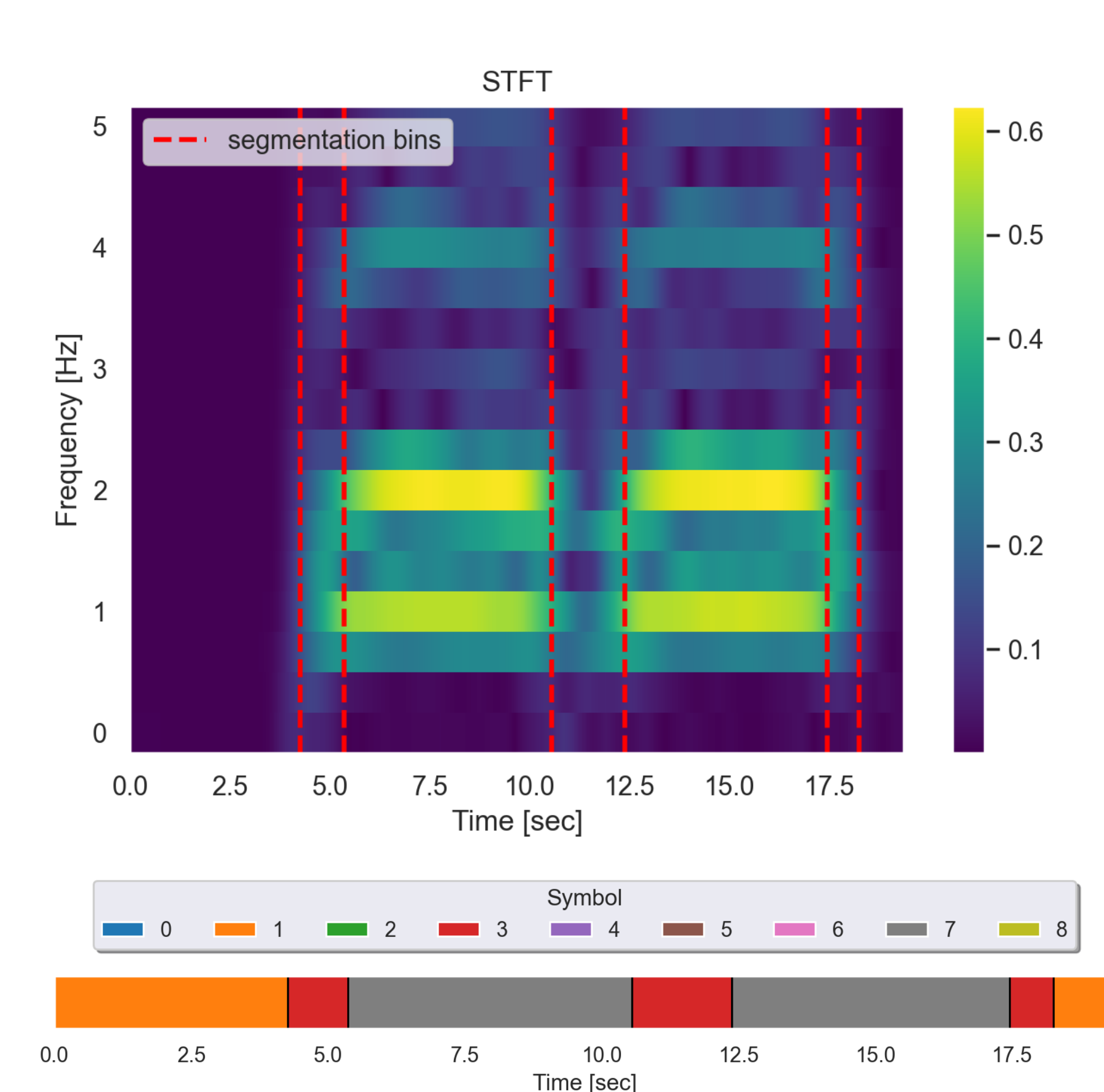


Figure 3: Spectrogram (multivariate signal) of one recording with its corresponding color bar.

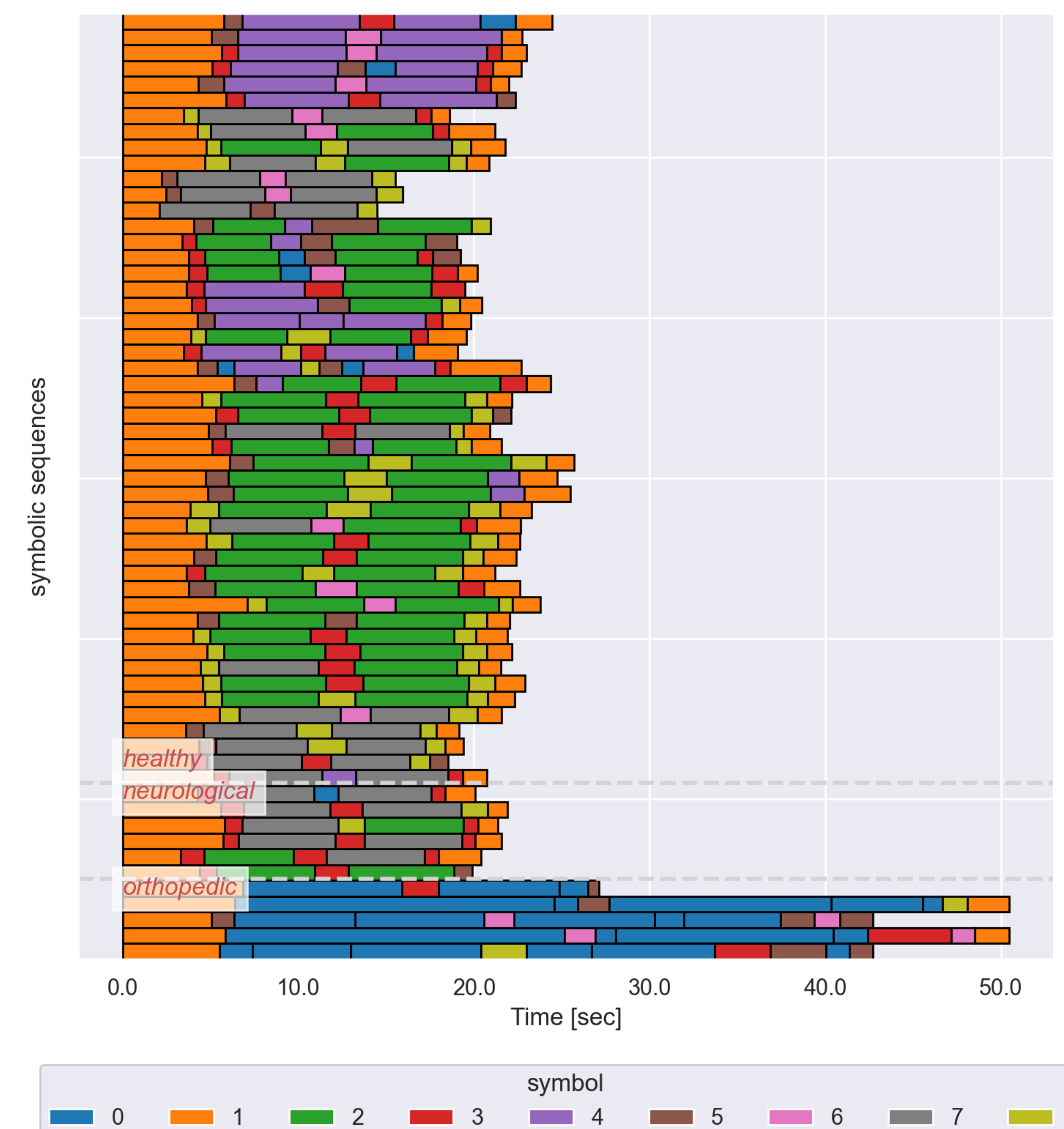


Figure 4: Color bars for 60 recordings, with 3 classes and  $A = 9$ .

## Experimental results: the distance

Silhouette coefficient calculated using the distance matrix and the ground truth patient group:

Distance measure	Mean Silhouette score	Median Silhouette score
DTW-D	0.15	0.18
DTW-I	0.15	0.19
$d_{symb}$	0.33	0.40

Robustness to the difference in lengths:

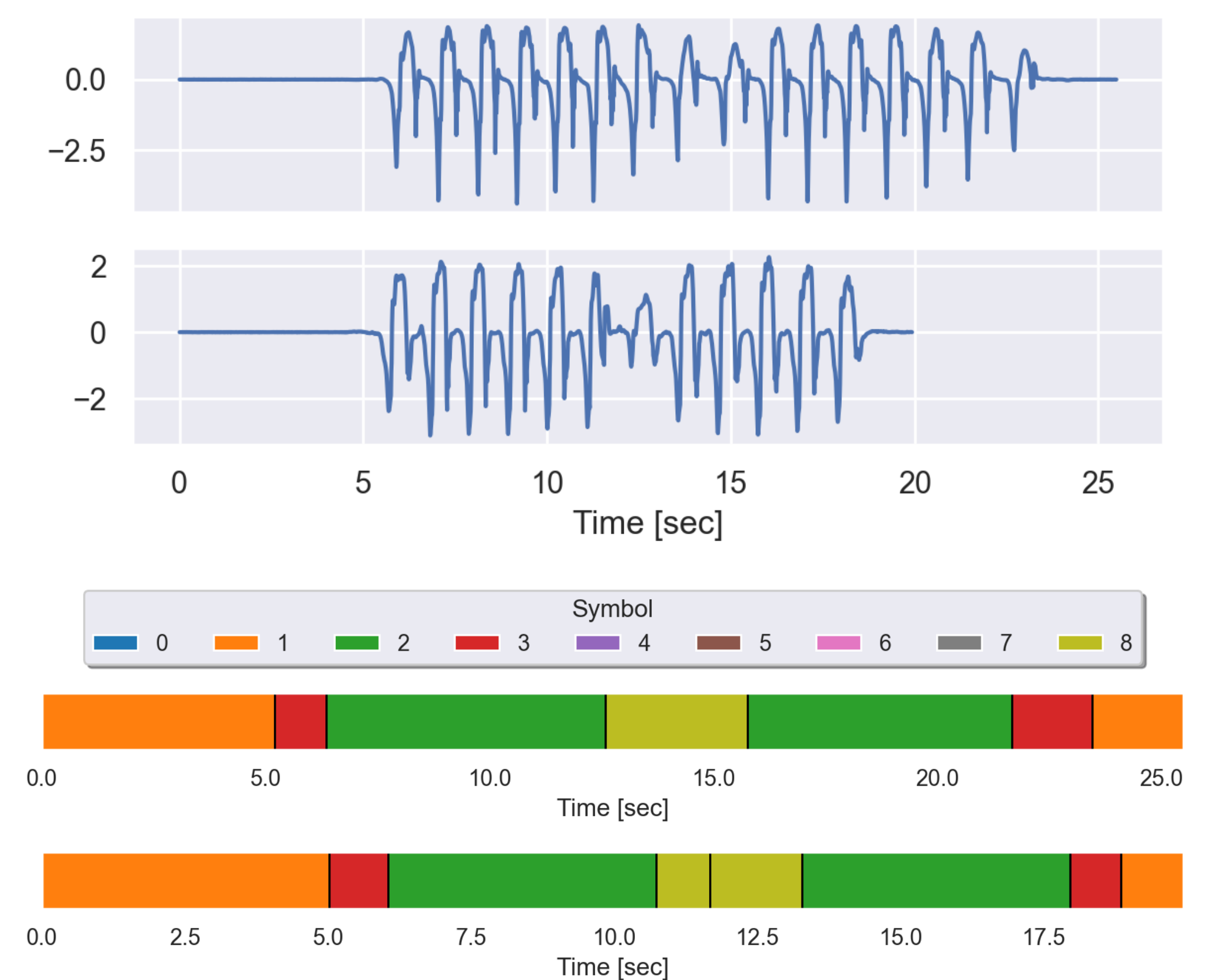


Figure 5: Two gait signals and their color bars.

## References

- [1] S. W. Combettes, C. Truong, and L. Oudre. An interpretable distance measure for multivariate non-stationary physiological signals. In *2023 IEEE International Conference on Data Mining Workshops (ICDMW)*, pages 533–539, 2023.
- [2] R. Killick, P. Fearnhead, and I. A. Eckley. Optimal detection of changepoints with a linear computational cost. *Journal of the American Statistical Association*, 107(500):1590–1598, 2012.
- [3] C. Truong and et al. A Data Set for the Study of Human Locomotion with Inertial Measurements Units. *Image Processing On Line*, 9:381–390, 2019. <https://doi.org/10.5201/ipo1.2019.265>.